

# **Full-Wave Simulation of an Optofluidic Transmission-Mode Biosensor**

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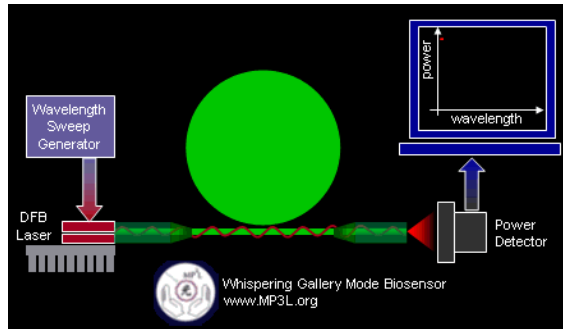
# Outline

- **Transverse Waveguide-based Biosensors**
- **Novel Optofluidic Biosensor**
- **Antiresonant Reflecting Optical Waveguides**
- **Device Simulation**
- **Conclusions**

# Transverse – Waveguide Based Biosensors

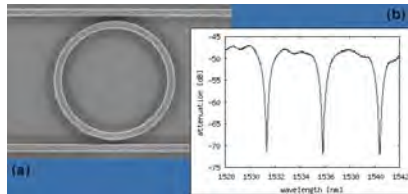


Whispering Gallery Mode Sensor



F. Vollmer et al. App. Phys. Lett. 80, 4057 -4059 (2002).

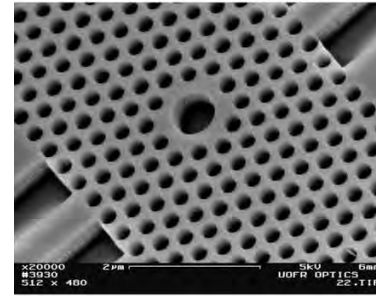
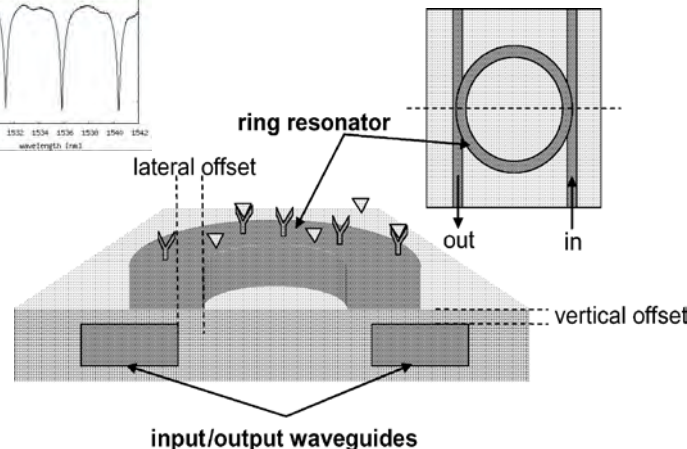
## Microring Resonator



Advantages:

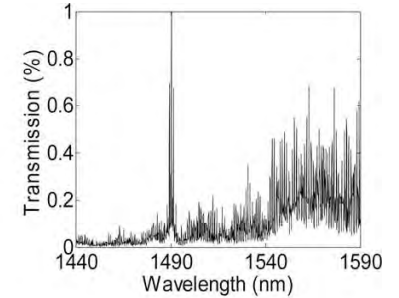
High Sensitivity

A. Yalcin et al. IEEE J. Sel. Topics Quant. Elec. (2006)

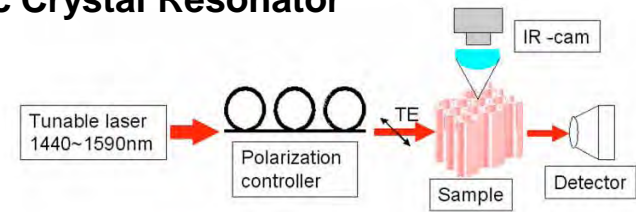


(a)

Photonic Crystal Resonator



(b)

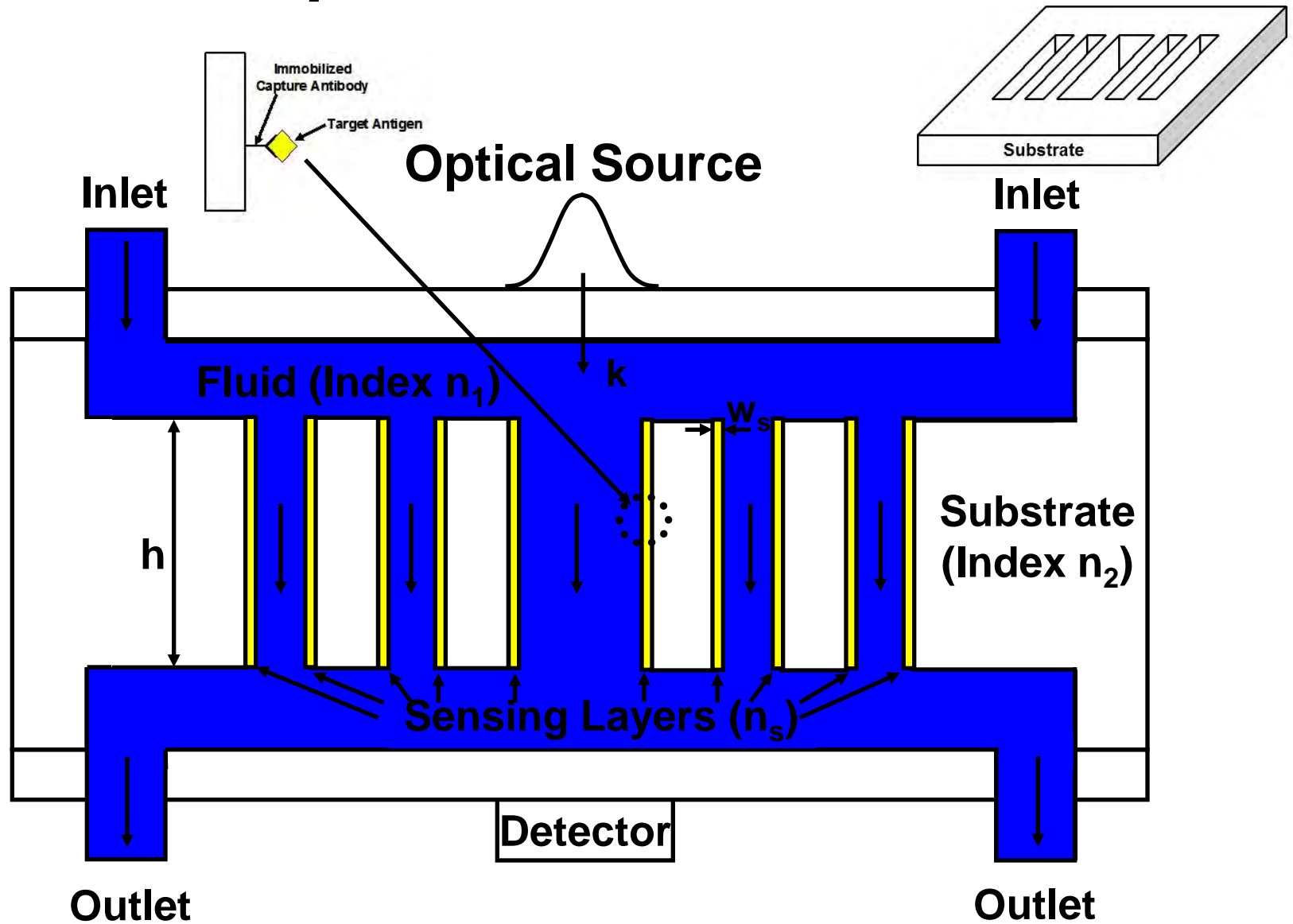


MR Lee and P. Fauchet, Opt. Exp. (2007)

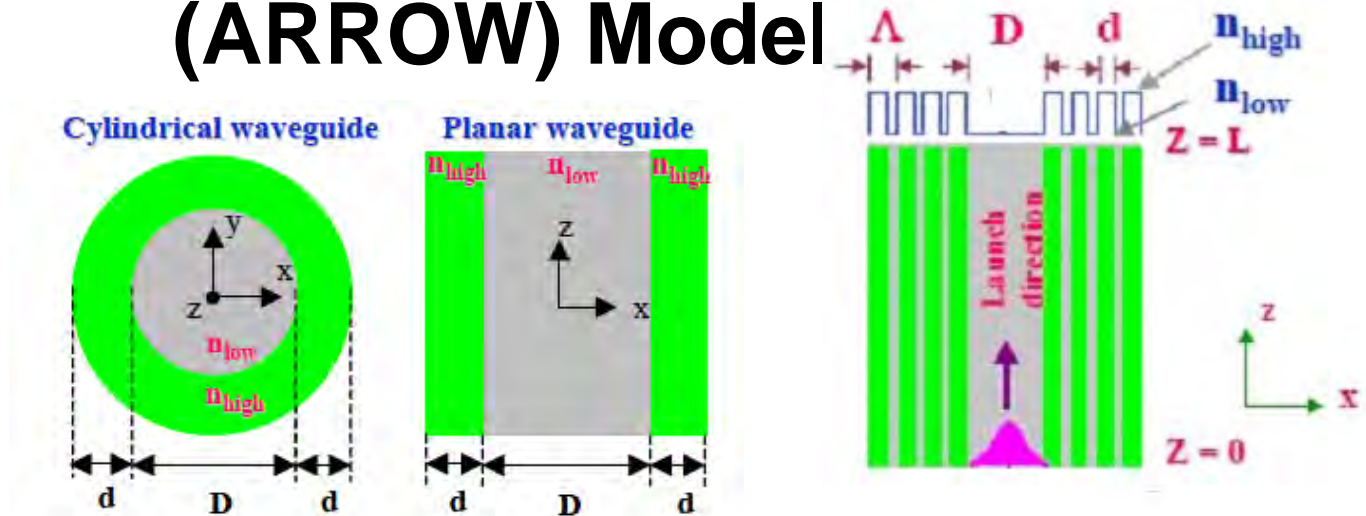
## Disadvantages:

- Difficult multiplexing for array applications
- Sensitive alignment coupling - awkward for POS applications

# Optofluidic Biosensor



# Antiresonant Reflecting Optical Waveguide (ARROW) Model



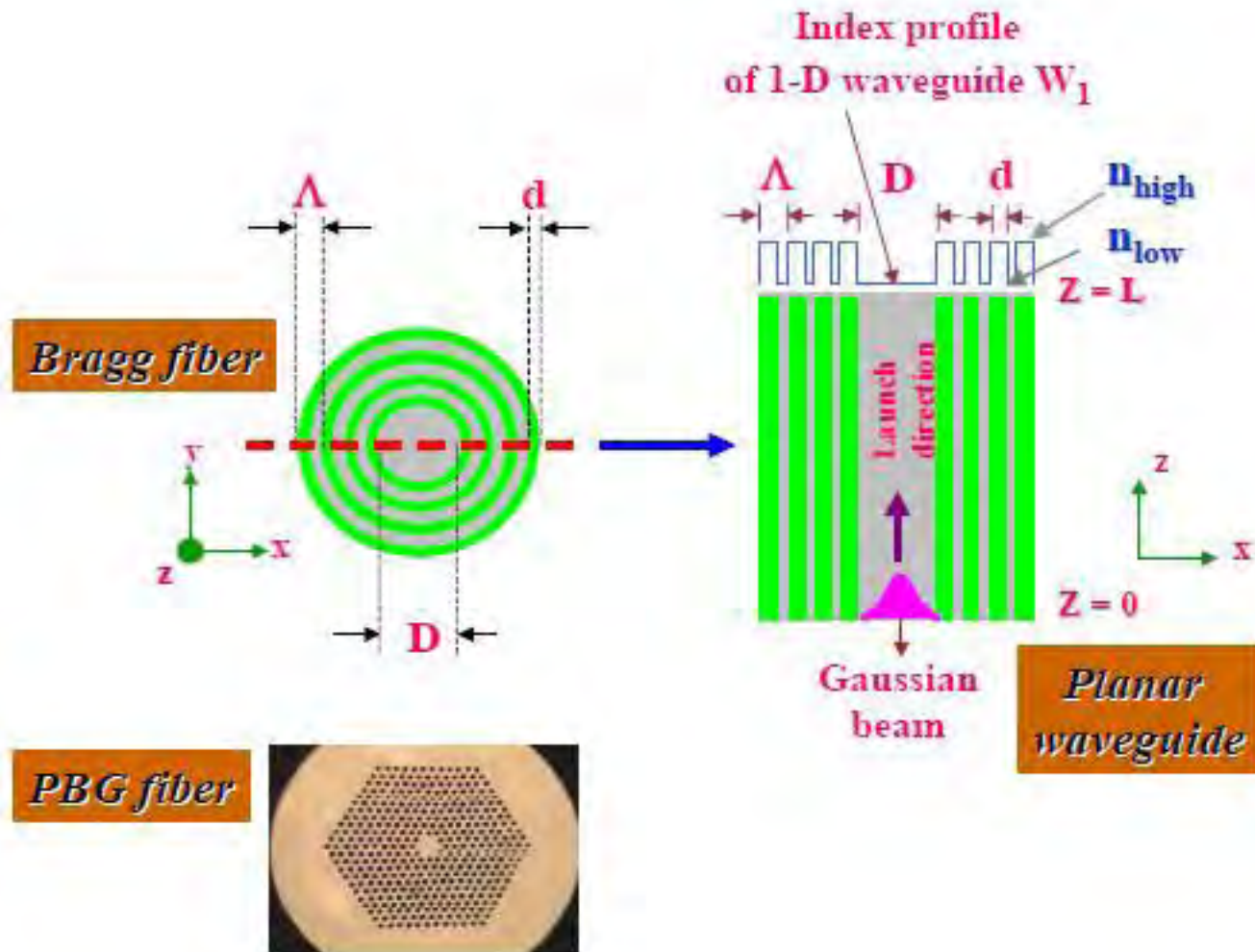
## Antiresonant Reflecting Optical Waveguide (ARROW) model

The high-index layer on either side of the low-index core behaves as a Fabry-Perot resonator in the ARROW model.

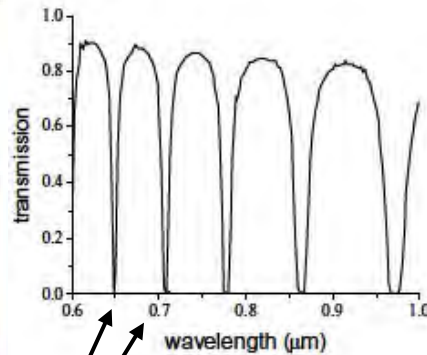
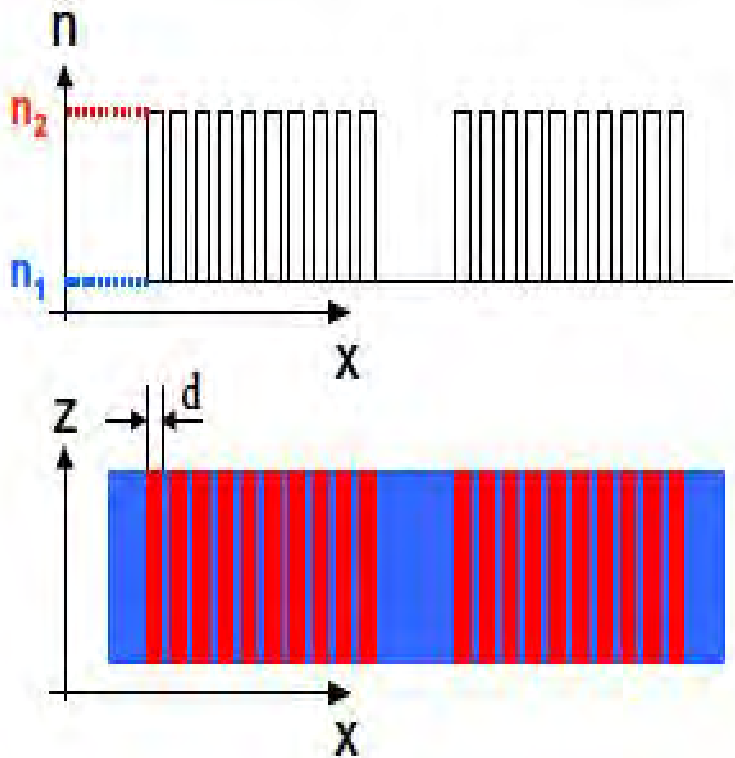
A standing wave builds up in the high-index layer when  $k_{ex}d = \pi m$ ,  $m = 1, 2, \dots$ , where  $k_{ex}$  is the propagation constant. This corresponds to a resonant condition in the high-index layer so that light leaks out of the core, thus giving rise to the transmission minima.

The transmission maxima result from antiresonant wavelengths that experience destructive interference within the high-index layer so that light is confined in the low-index core.

# Microstructured Optical Fibers

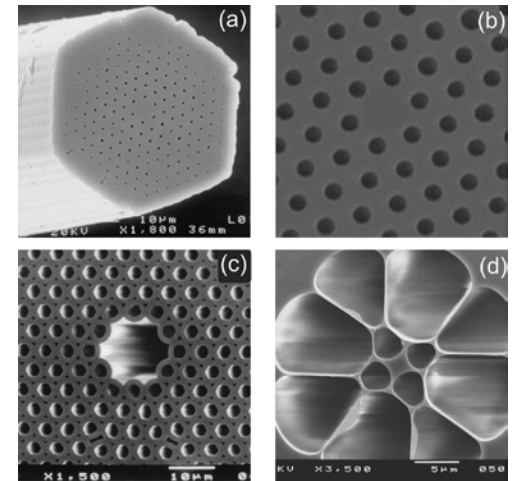
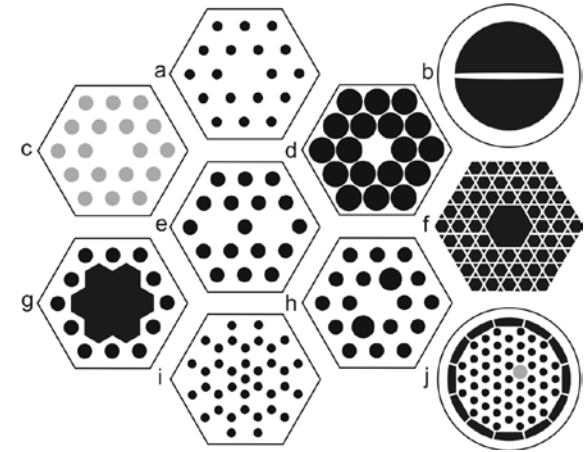


# Microstructured Optical Fiber (MOF) (Photonic Crystal Fibers)



Transmission Minima  $\lambda_m$

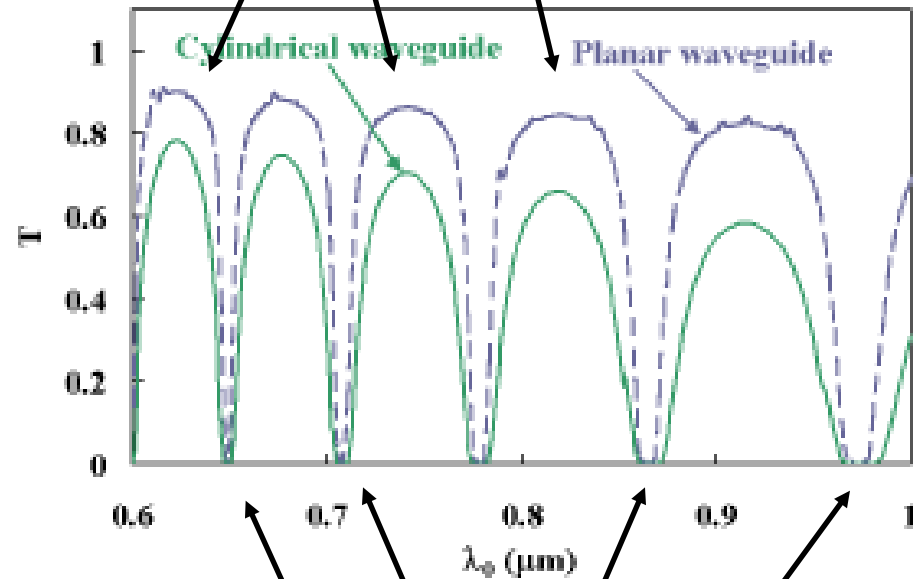
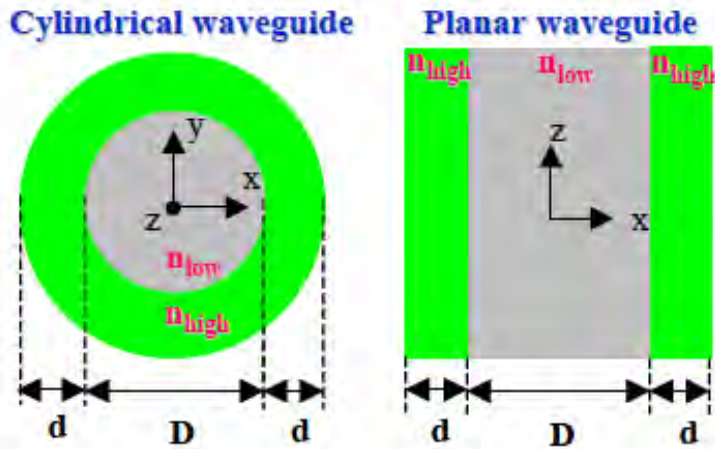
$$\lambda_m = \frac{2n_1d}{m} \left[ \left( \frac{n_2}{n_1} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 1, 2, \dots)$$



# Analysis of Transmission Spectrum

## Antiresonant Reflecting Optical Waveguide (ARROW) model

**Maxima**  $\lambda_l = \frac{4n_{low}d}{(2l+1)} \left[ \left( \frac{n_{high}}{n_{low}} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (l = 0, 1, 2, \dots)$



Analytical analysis applies when

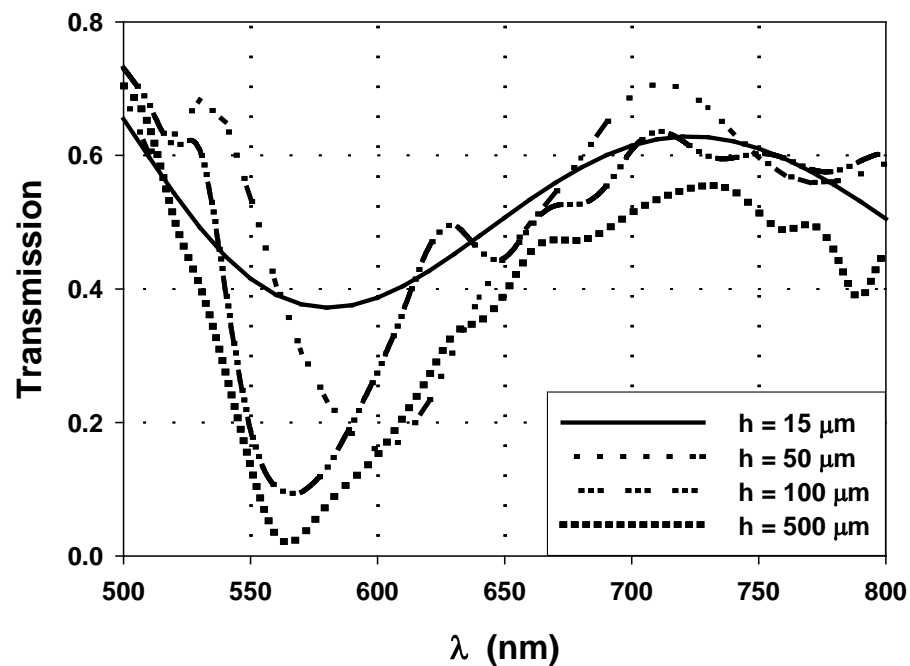
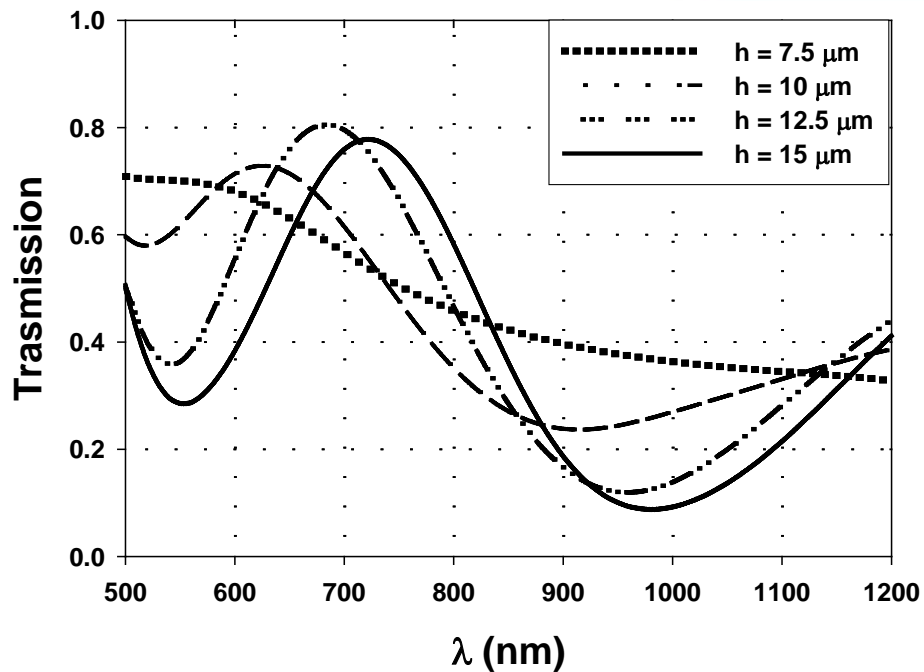
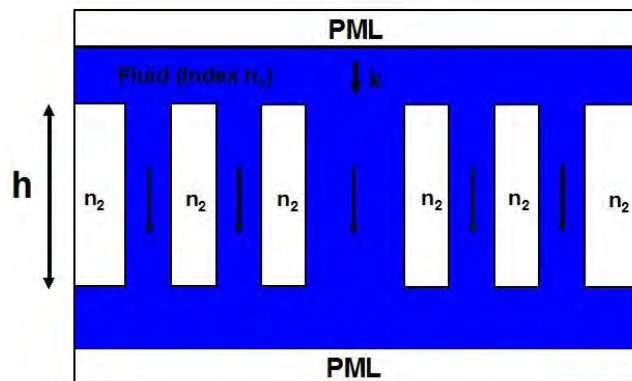
$$\frac{\lambda}{D} \ll 1$$

**Minima**  $\lambda_m = \frac{2n_{low}d}{m} \left[ \left( \frac{n_{high}}{n_{low}} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 1, 2, \dots)$



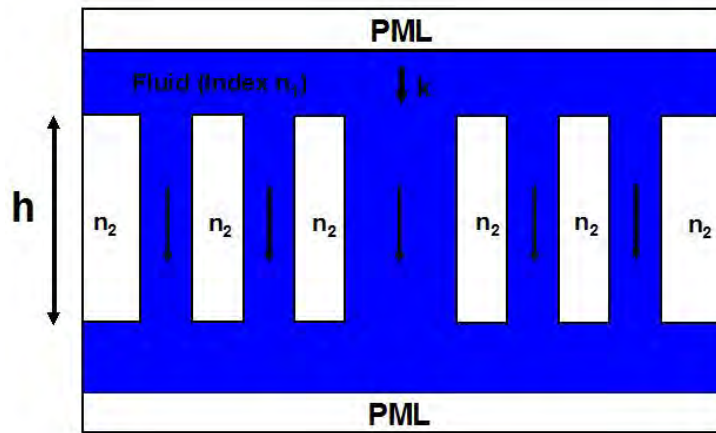


# Transmission Spectra vs. Substrate Thickness ( $h$ )

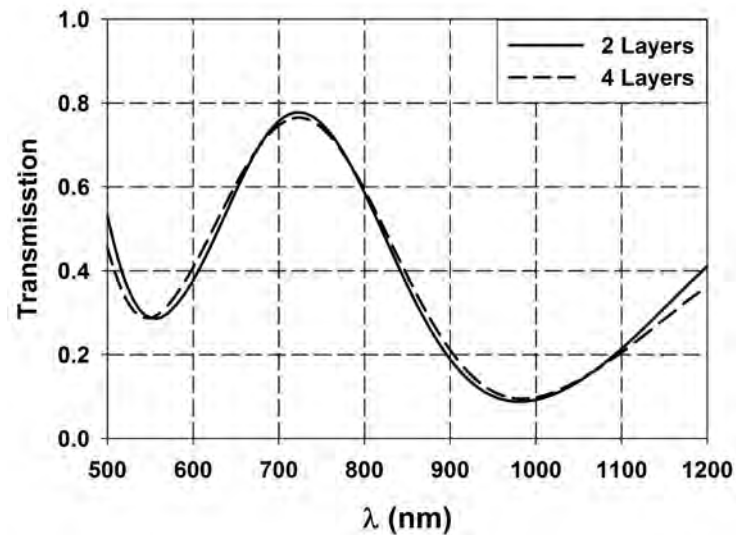
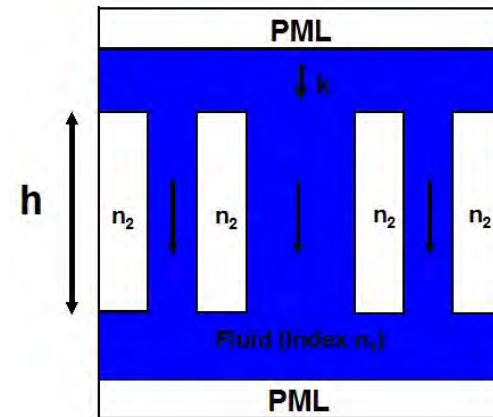


# Transmission vs. Number of Layers

## Four Layers



## Two Layers

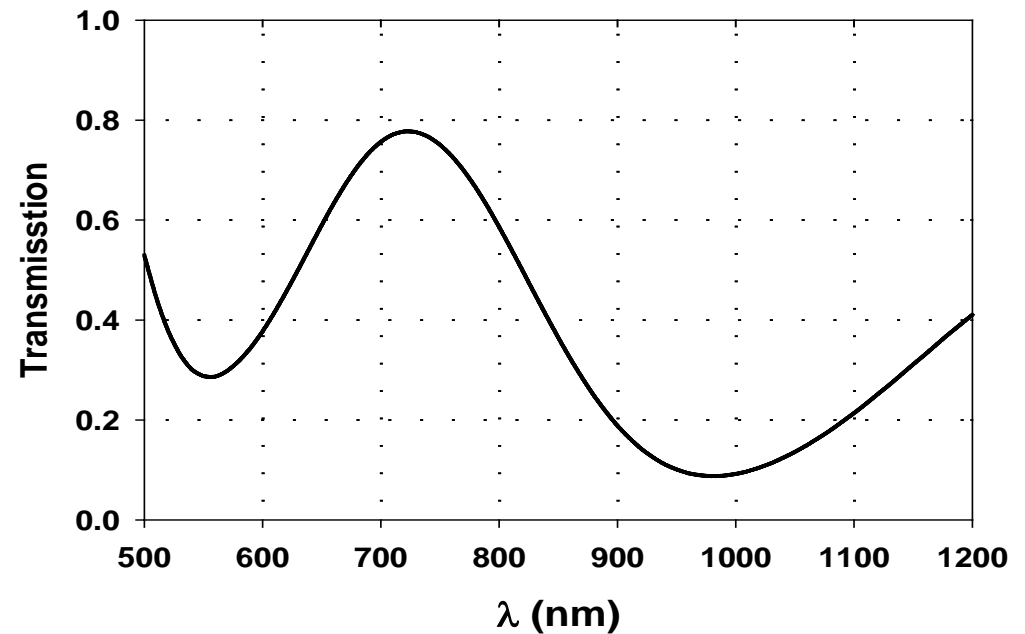
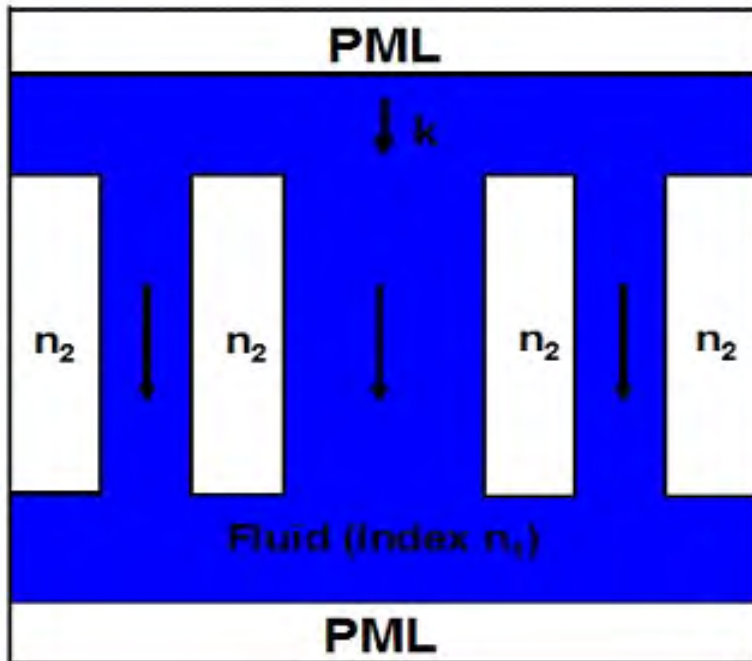


# Time-Harmonic Full-Wave Analysis

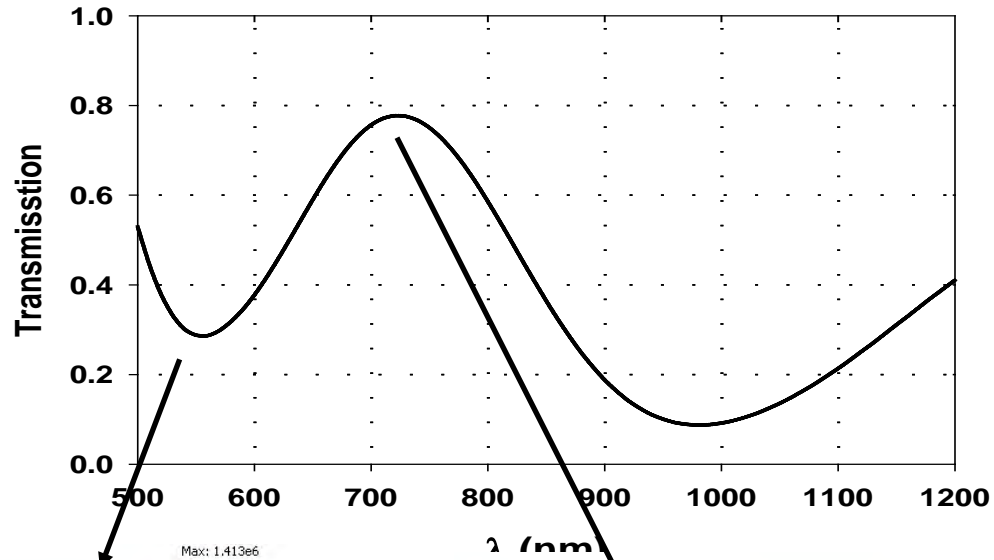
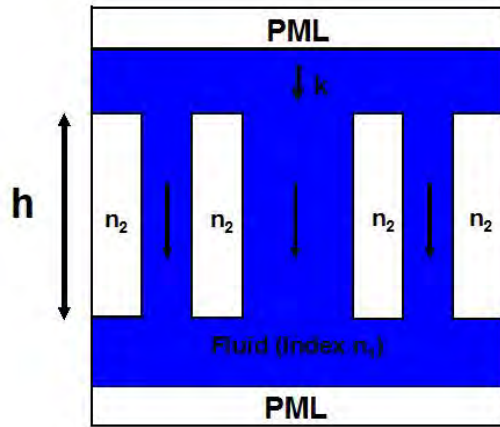
## Device Design

Reduced Computational Domain  
Mesh: 48,306 cubic elements

Parametric Analysis: It takes approximately 15 min to compute a transmission spectrum using a dual quad-core workstation (Windows XP 64 bit) with 24 GB of RAM

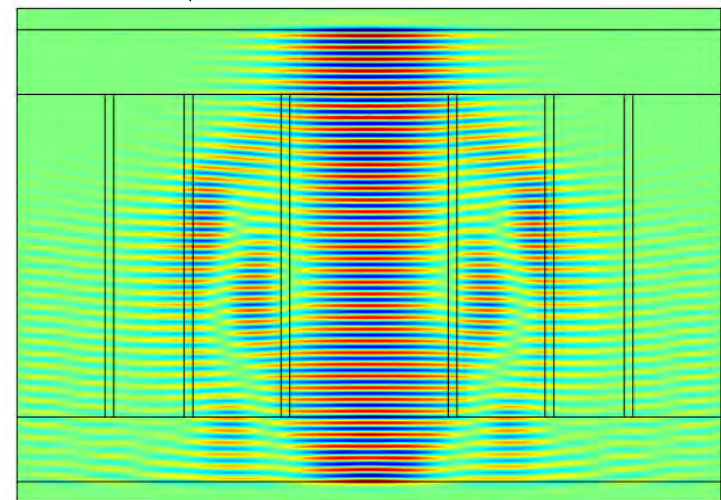
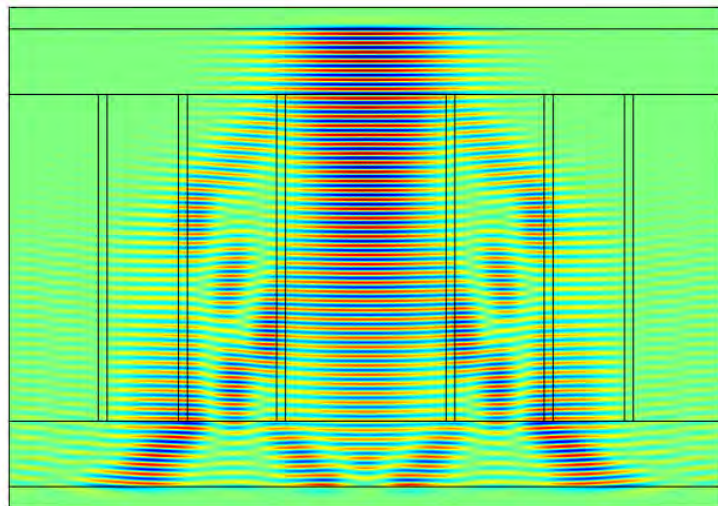


# Analysis of Transmission Spectrum

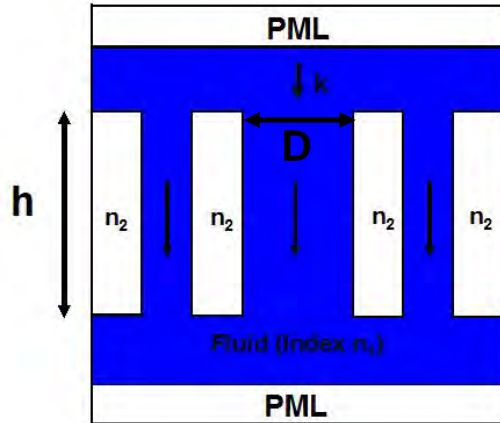


$\lambda = 560$  nm

$\lambda = 720$  nm

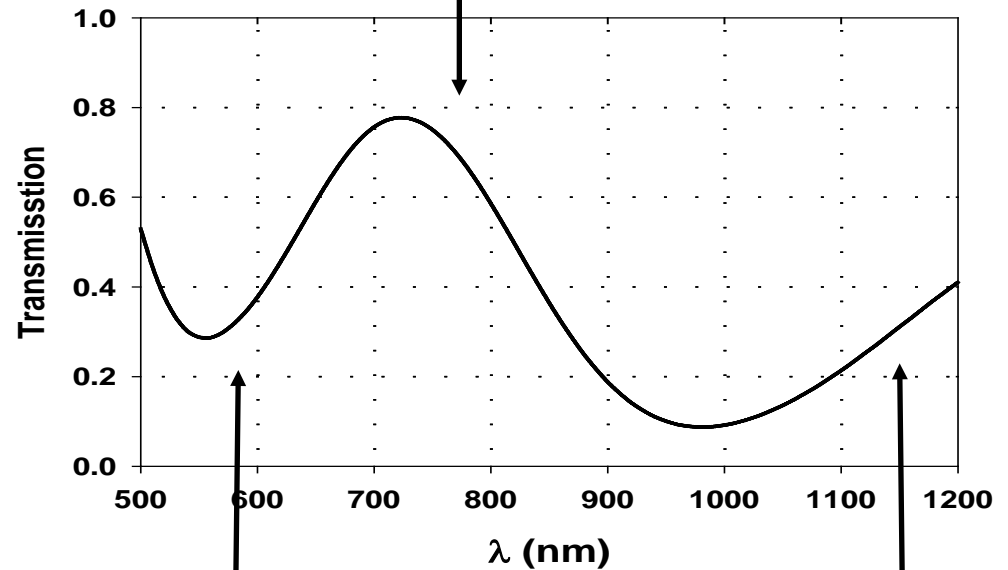


# Comparison with Analytical Analysis



**Maxima** 
$$\lambda_l = \frac{4n_{low}d}{(2l+1)} \left[ \left( \frac{n_{high}}{n_{low}} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (l = 0, 1, 2, \dots)$$

$\lambda_{1,max} = 770 \text{ nm}$        $\lambda_{0,max} = 2310 \text{ nm}$



Analytical analysis applies when  $\frac{\lambda}{D} \ll 1$

$d = 1 \mu\text{m}$

$n_1 = 1.33 \text{ (H}_2\text{O)}$

$n_2 = 1.45 \text{ (SiO}_2\text{)}$

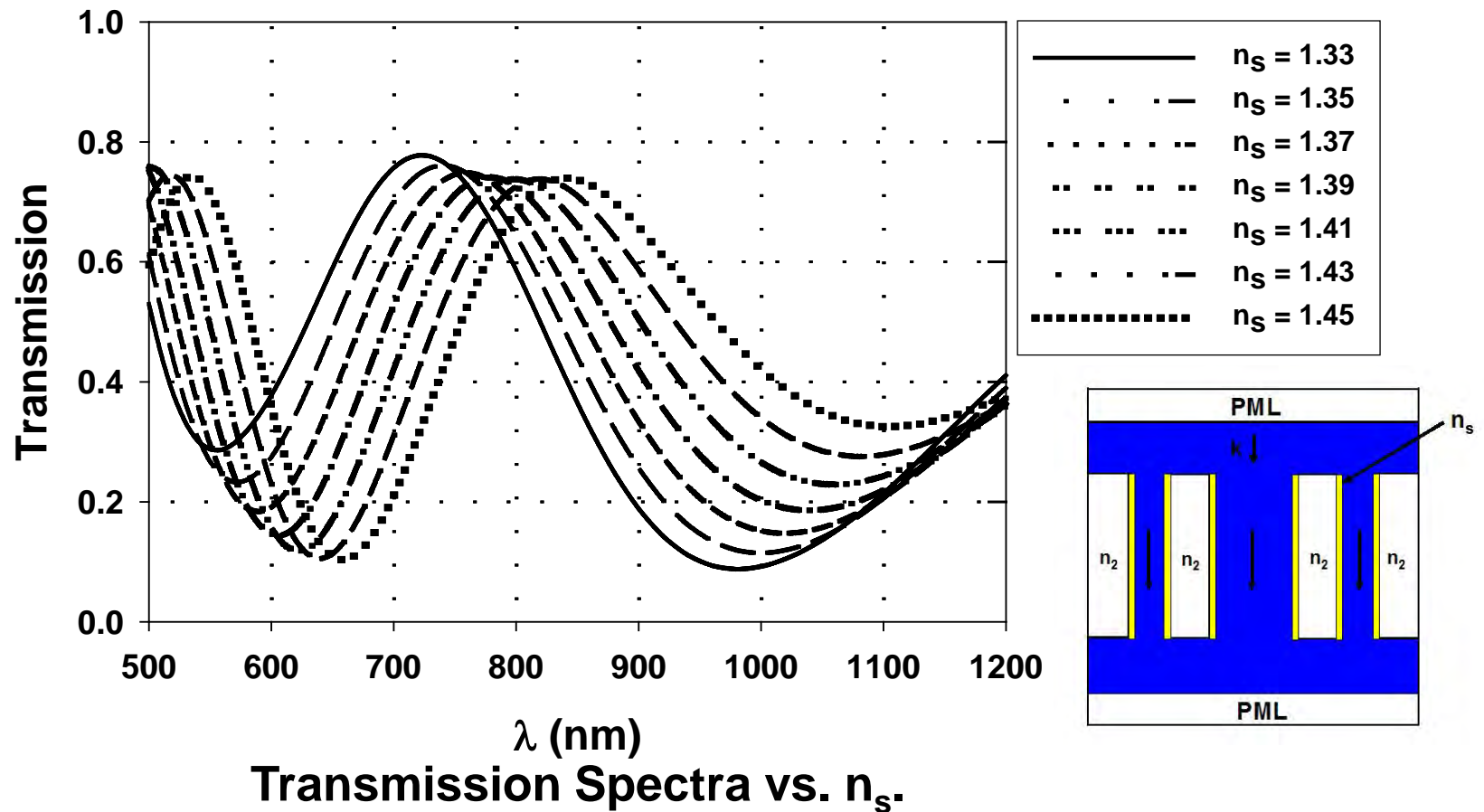
**Minima**

$$\lambda_m = \frac{2n_{low}d}{m} \left[ \left( \frac{n_{high}}{n_{low}} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 1, 2, \dots)$$

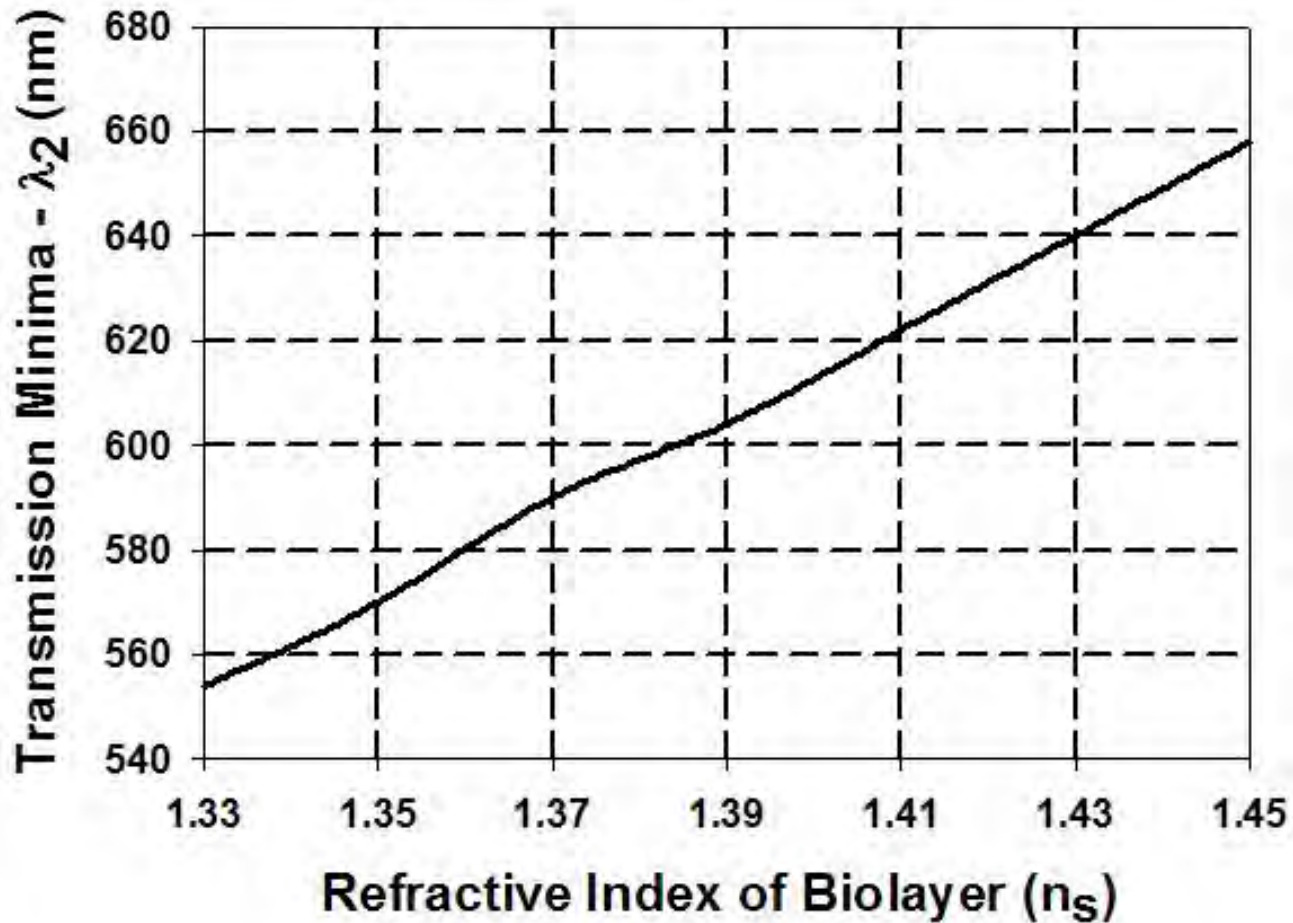
$\lambda_{2,min} = 578 \text{ nm}$

$\lambda_{1,min} = 1155 \text{ nm}$

# Transmission Spectra vs. Refractive Index of Sensing Layer $n_s$

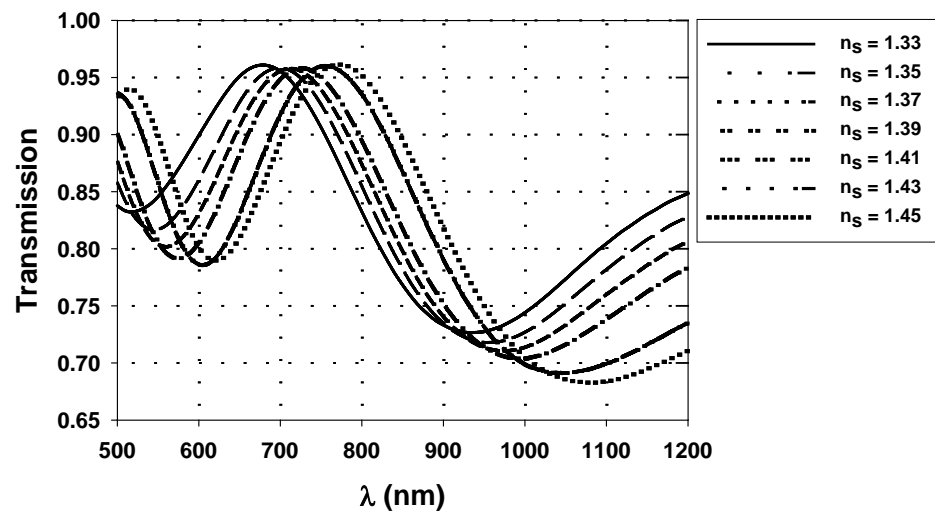
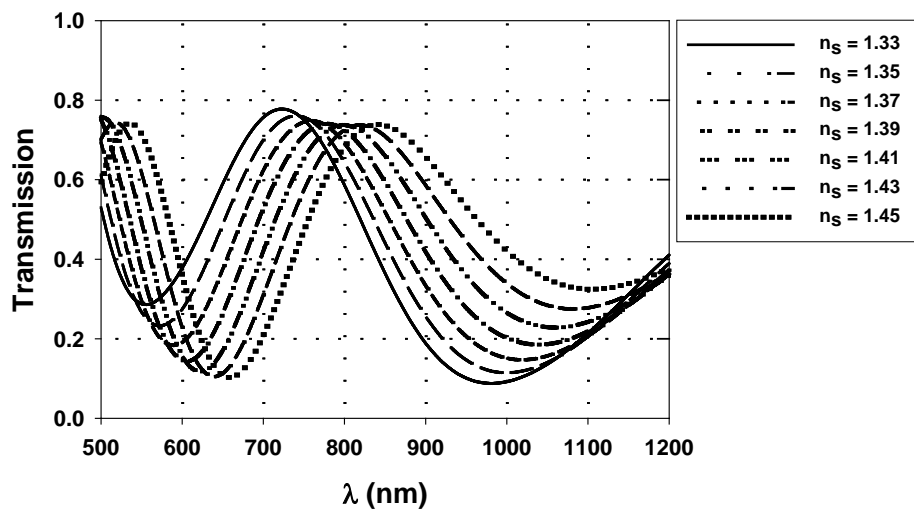
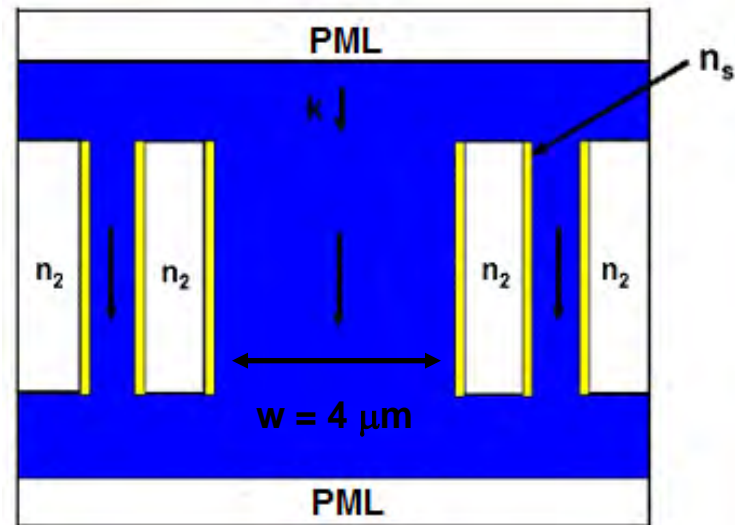
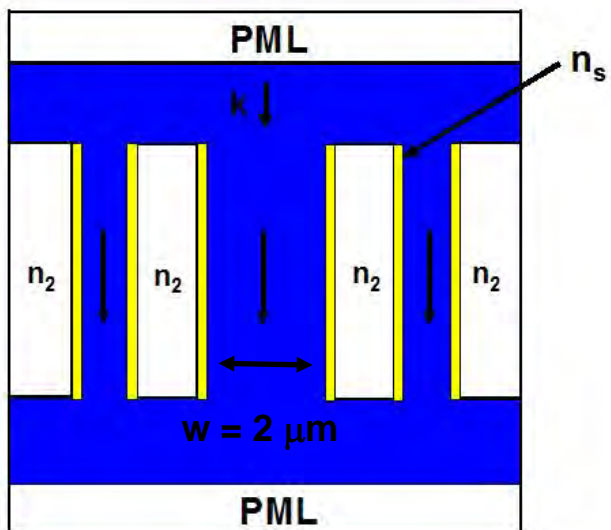


# Shift in $\lambda_2$ Transmission Minima vs. Refractive Index of Sensing Layer $n_s$





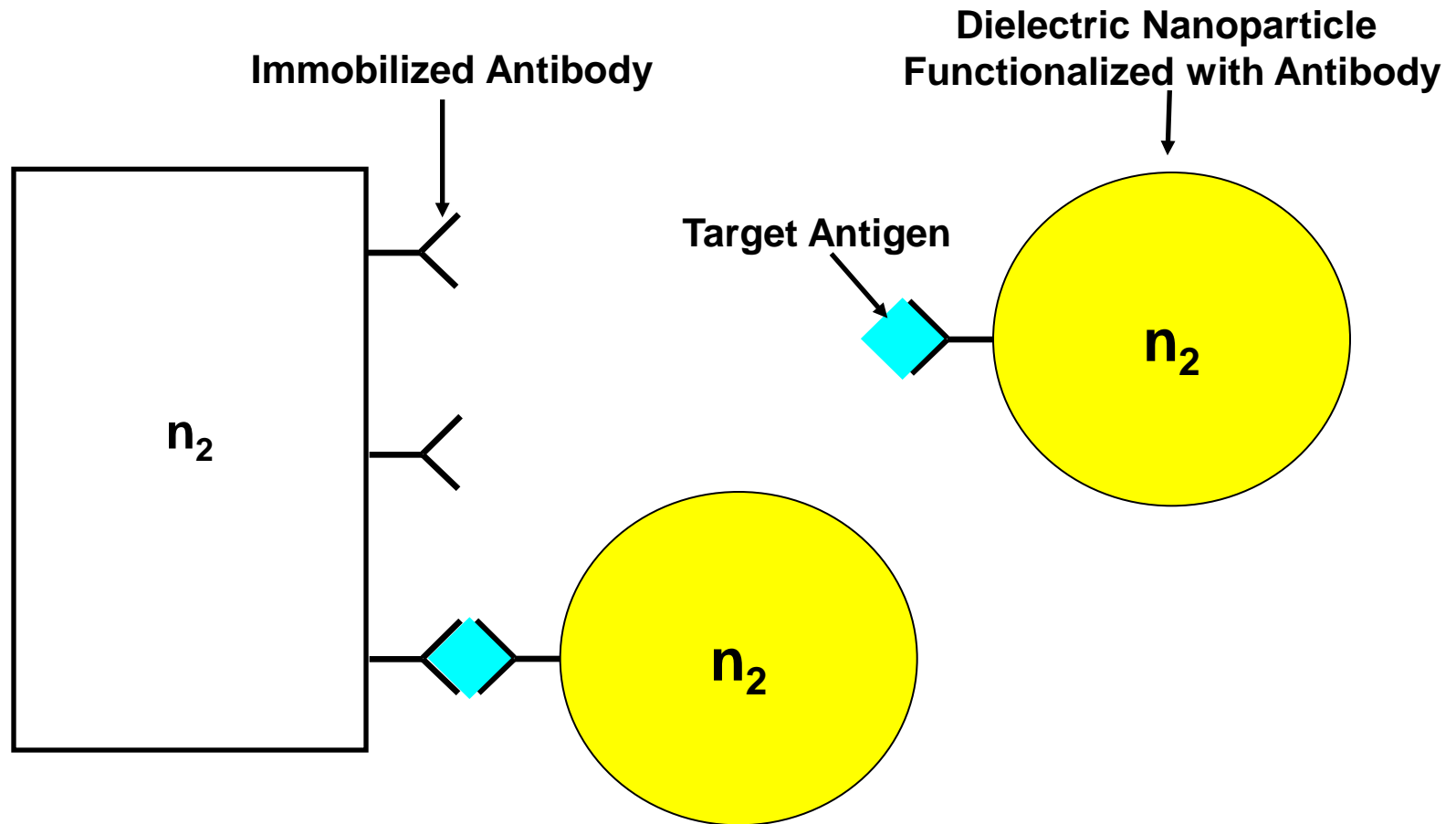
# Transmission vs. Channel Width



# Detection Sensitivity

(Spectral Shift vs. Biolayer Thickness  $w_s$ )

## Nanoparticle-Based Immunoassay



# Sensitivity – Spectral Shift vs. Biolayer Thickness $w_s$

## Transmission Minima

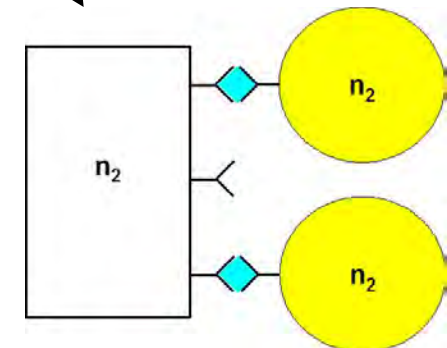
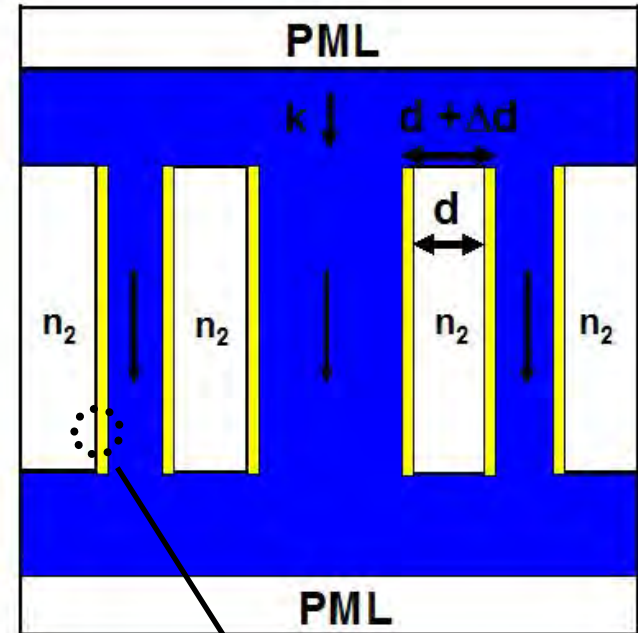
$$\lambda_m = \frac{2n_1 d}{m} \left[ \left( \frac{n_2}{n_1} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 1, 2, \dots)$$

$$\Delta\lambda_m = \frac{2n_1 \Delta d}{m} \left[ \left( \frac{n_2}{n_1} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 1, 2, \dots)$$

$$\Delta\lambda_2 = n_1 \Delta d \left[ \left( \frac{n_2}{n_1} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 2)$$

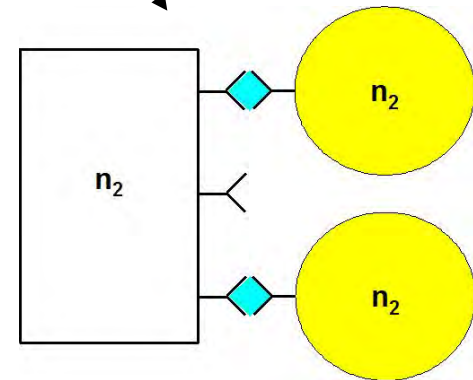
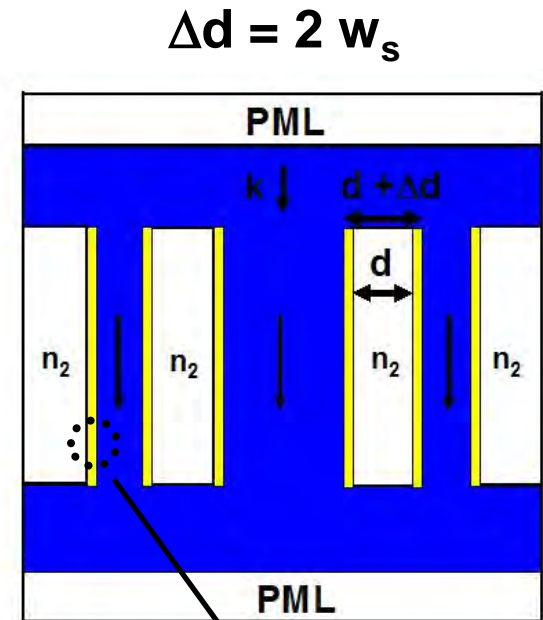
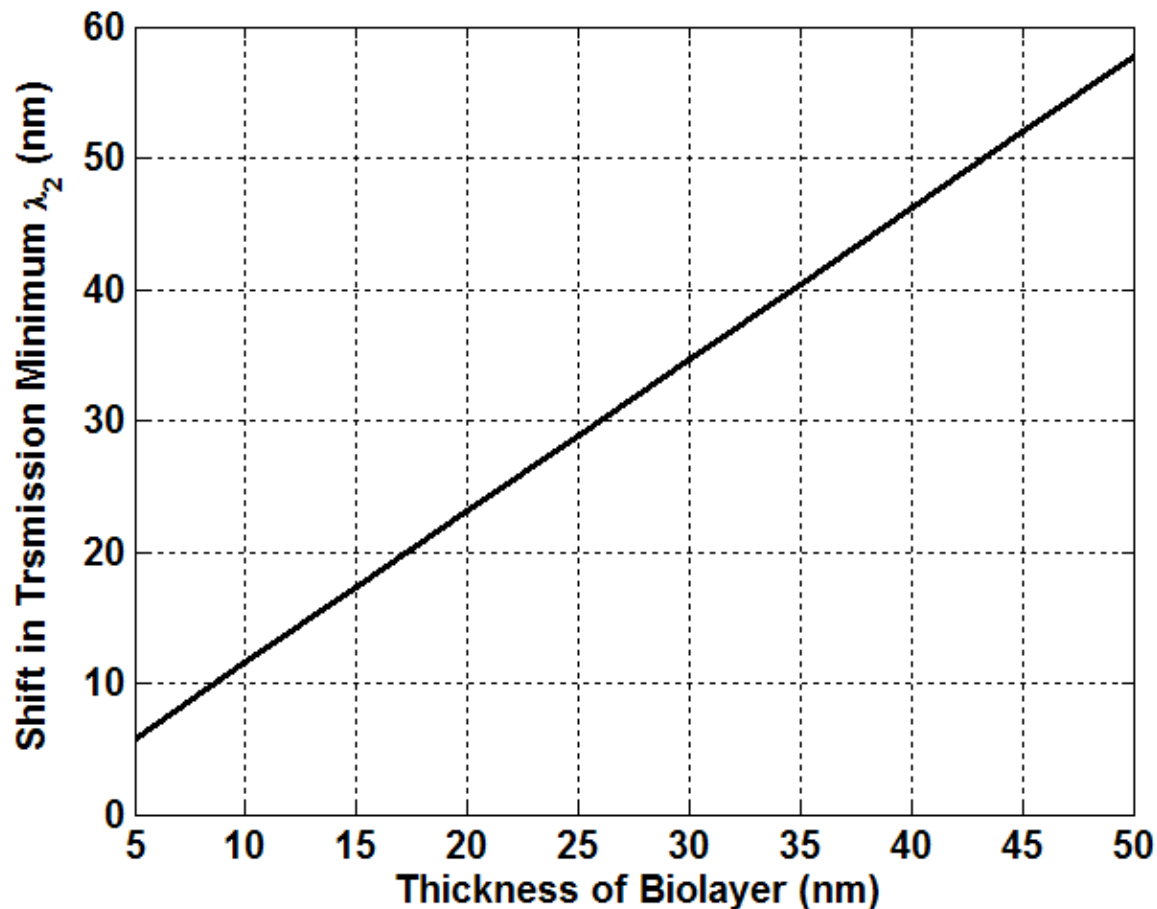
$$\Delta\lambda_2 = 2n_1 w_s \left[ \left( \frac{n_2}{n_1} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 2)$$

$$\Delta d = 2 w_s$$



# Sensitivity – Spectral Shift vs. Biolayer Thickness $w_s$

$$\Delta\lambda_2 = 2n_1w_s \left[ \left( \frac{n_2}{n_1} \right)^2 - 1 \right]^{\frac{1}{2}} \quad (m = 2)$$



# Conclusions

- **Introduction of a novel Optofluidic Transmission- Mode Biosensor.**
- **Biosensing based on contrast in refractive index between target biomaterial and carrier fluid.**
- **The presence of target biomaterial causes a detectable shift in transmission spectrum of sensor.**
- **Transmission mode operation facilitates array sensing with potential for multiple target antigens detected on a single chip.**
- **Device design and optimization can be completed in a few days using Comsol RF solver,**
- **Sensor architecture holds potential for low cost POS clinical diagnostic applications.**